The Mechanism Underlying Heart Rate and Pacemaking Activity Decline in Developing Sinoatrial Node of the Rabbit Heart

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Abstract

Diagnosis of heart disease and its treatment are based largely on our understanding of the electrophysiology of adult myocardium. However, the marked difference in the electrical action potential (AP)between neonatal and adult cardiac myocytes suggests a different set of molecular bases in neonatal myocytes, and therefore different treatment for new-borns. In this study we present a new mathematical model of sinoatrial node (SAN) cells of the neonatal rabbit ,by modifying densities or kinetics of I_{Na}, I_{CaL}, I_f, I_{Kr}, I_{Ks}, and I_{NaCa} in the adult rabbit SAN cell models developed by Zhang et al., based on available experimental data obtained from new-born rabbit SAN cells. The new model reproduced APs similar to experimental recordings from neonatal myocytes, with a faster pacemaking rate. Using the new model, we investigated how age-related changes in ionic currents modulate pacemaking AP morphology, demonstrating the model as a useful tool for testing the effects of drugs on neonatal SAN cells to obtain a better quantitative understanding of differences between neonatal and adult physiology.

1.Introduction

The function of the heart is compromised during maturation in many species leading to a decrease in the heart rate (HR)[1]. Experimental studies have shown that there are significant developmental changes in the expression and function of ion channels and other cellular elements, leading to a postnatal alternation in the spontaneous pacemaking activity of the transmembrane potential in isolated rabbit SAN cells [2]. This may be responsible for the observed differences in the automaticity and characteristics of the membrane potentials in the adults as compared to the neonatal hearts, including a reduction in spontaneous beating rate, an increase in action potential duration (APD), the intrinsic cycle length(CL), and an increased maximal diastolic potential (MDP)[2].

In this study, we attempted to provide a modelling framework to underpin the ionic mechanism for the developmental maturation of the rabbit SAN at the single cell level based on combined experimental findings on channel properties and gene expression of the ion channel currents and intracellular calcium handling. Using the model we investigated how the remodelling in the expression and function of different ion channels and other intracellular Ca2+ handling contribute to the alteration of the pacemaking activity of the SAN cells, resulting in the slowing down of the heart rate in the adult heart.

2.Methods

Based on the adult rabbit SAN cell model developed by Zhang *et al.*[3], we modified the formulations of ionic currents and their current densities of the model to incorporate experimental data obtained from neonatal rabbit SAN cells. The main changes made to the Zhang *et al.* [3] model are summarized as follows.

2.1.Fast sodium current, I_{Na}

I_{Na} was described using a Hodgkin-Huxley formulations, which were incorporated into the Zhang *et al.* model based on experimental data from Brousticci *et al.*[4]of both new-born and young rabbit SAN cells. The activation and inactivation steady state curves of the model were fitted to the experimental data of Baruscotti *et al.*[4], with a shift to the $V_{1/2}$ of the activation curve (as seen in Figure1A), considering the experimental data were obtained at room temperature 20°C while the model was developed for the body temperature. In addition, aQ$_{1O}$ correction of the current density was also considered accounting for the temperature difference. To validate the model, simulated voltage-clamp data of I_{Na} were compared to experimental data. In the voltage clamp simulation, I_{Na} was computed from a holding potential of -60 mV, which

was followed by a series of test potentials lasting 10 ms, varying from -60 mV to 45 mV with a 5mVincrement. The maximal channel conductance of the sodium current, $g_{Na,max}$, was determined by reproducing the experimental data on the *I-V* relationship as represented in Figure 1B.Based on the experimental data, the peak I_{Na} current density of the neonate *I-V* curve was greater than that of the young. This resulted in a relatively larger "window current" seen in the neonate case [4]
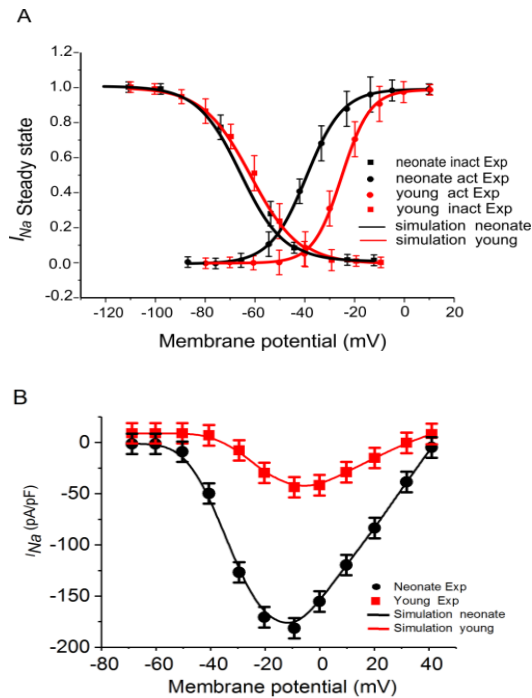

Figure 1.(A) Steady state activation and inactivation curves of the I_{Na} current in neonate and young age groups. Modelling date fits to experimental data.(B)Simulated *I–V* relationship between the two age group, which were validated against experimental data from Brousticci *et al.*[4].

2.2.L-type calcium current, $I_{Ca,L}$

The $I_{Ca,L}$ formulation used in Zhang *et al.*[3]model was modified based on the available experimental data from Protas *et al.*[5]for the neonate SAN cells. The steady state activation and inactivation curves were fitted to the experimental data, but with a 5 mV rightward shift to the V1/2 of the inactivation curve and a 5 mV leftward shift to the V1/2 of activation curve in the adult, resulting in an increased I_{CaL} window current for the adult cells as seen in Figure 2A. Using voltage clamp protocol as used in experiments (with a holding potential of -50 mV, which was followed by a series of test potentials lasting 300 ms, varying from -50 mV to 50 mV with a 10mV increment),

$I_{Ca,L}$ was computed and the established *I-V* relationship curve of $I_{Ca,L}$ on neonate and adult rabbit SAN cells were validated against experimental data[5] as illustrated in Figure2B.
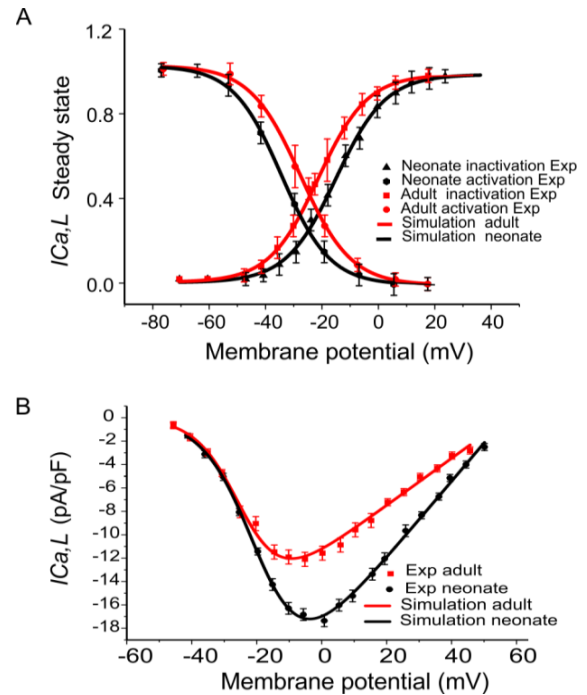

Figure2.(A)Fitted steady state activation and inactivation gate curves of $I_{Ca,L}$ in two neonate and adult age groups.(B) Simulated *I–V* relationship of the two age group, which were validated against experimental data by Protas *et al.*[5].

2.3.Funny current, I_f

The formulation of I_f in the Zhang *et al.*[3]model was modified based on the available data by Accil *et al.*[6]and Yang *et al.*[7]. The activation curve was fitted to experimental data with an age-related negative shift of the activation $V_{1/2}$ by 7mv (as shown in Figure3A). It was also shown that the If current density is greater in the neonate than in the adult SAN cells, with an increase of the maximal conductance of g_{Na}, $g_{f,K}$ by 70% in the neonate as compared to the adult cells. . The simulated *I-V* curve (Figure3B) was validated against experiment data by Protas *et al.*[8]and Honjo *et al.*[9].

2.3.Other ion currents

Other ion channel currents including I_{Kr}, I_{Ks}, and I_{NaCa} were modified on the basis of changes in the expression of ion channels and Ca^{2+}-handling proteins during development as a previous quantitative PCR, *insitu*

hybridization and immunohistochemistry study investigated[10]. This was done through modification of the maximal conductance of g_{Kr} by 60%, g_{Ks} by 25% and K_{NaCa} by 50% in the Zhang *et al.* [3] model
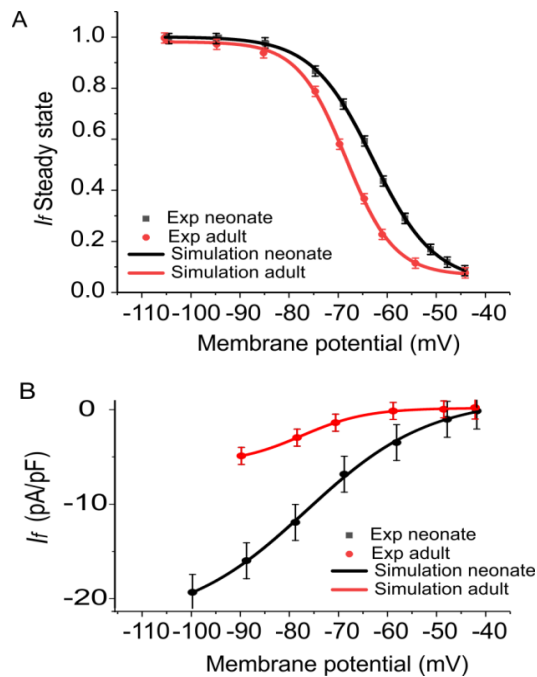
Figure3.(A) Fitted steady state activation curves of the I_f current in the neonate and adult age groups. (B) Simulated $I–V$ relationship, which was validated against experimental data by Protas *et al.*[8]and Honjo *et al.* [9].

3.Results

Models of the pacemaking action potentials for the neonate and adult SAN cells were developed by incorporating the age-related remodelling of different ion channels (I_{Na}, $I_{Ca,L}$, I_f, I_{Kr} and I_{Ks} as well as I_{NaCA}) and calcium handling into the Zhang et al. (3) model as a basal adult SAN single cell model. Figure 4 illustrates the simulated AP of the neonate SAN cell, which is compared to that of the adult. It was shown that the neonate model reproduces APs with their shape and characteristic matching to experimental data. Mainly the neonatal APs have faster spontaneous activities, shorter durations and greater amplitudes as compared to those of the adult. The computed CL (i.e. the time interval between two successive pacemaking APs) of the neonate was 277 ms, which was markedly smaller than that of 327 in CL in the adult, showing an 18% prolongation of the CL due to age(as shown in Figure4B). This is quantitatively consistent with the experimental observation [10], which showed that the heartbeat of rabbits was slowed down during postnatal development by15%.Heart rate has been measured as around 230±50 bpm for neonates [10],[11], which is very close to our simulation data of 217 bpm in neonates and 160 bpm in adults(Figure 5B)respectively.
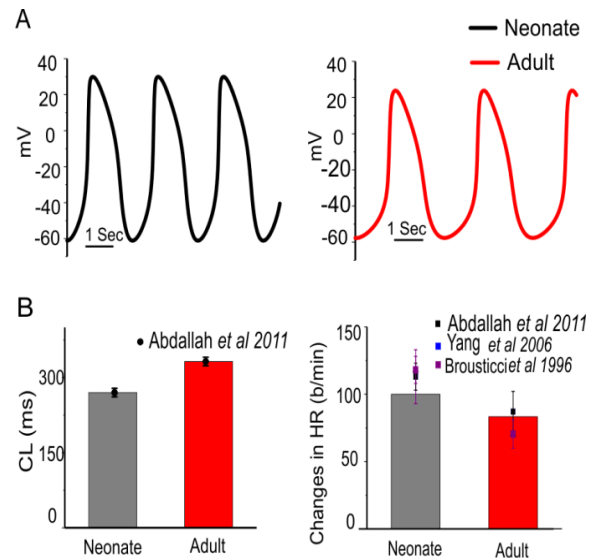
Figure4. (A) Simulated pacemaking action potentials in the neonate (black lines) and the adult (red lines) SAN cells. (B) Comparison of CL (right), HR (left) between the two age groups, which were validated by experimental data.

4.Discussion

The simulation result confirmed that there was an age-dependent change in the AP characteristics and pacemaking rate, causing a decreased SAN pacemaking activity in the adult. This finding indicates that the fast AP of the neonatal group results from changes in the balance of ionic currents that activate during the diastolic depolarisation phase compared to the adult group. A previous study[4] has reported that I_{Na} was present in rabbit central SAN cells at birth. The observation of this ion current during development showed that by the 40th postnatal day, the I_{Na} had fully disappeared. It was found neonate cells of central SA node exhibited a noticeable window current, resulting in the likely higher availability of sodium current in the diastolic depolarisation phase in neonates. With development, the $V_{1/2}$of the activation curve shifted in the positive direction, while the inactivation remained unaltered, resulting in a reduced overlap of the two curves and hence less window current. This decline in the window currents may help to explain how the principal current disappears gradually with age to become non-existent in adult SAN and be replaced by $I_{Ca,L}$.

The $I_{Ca,L}$ current was identified as the primary pacemaking current which initiates the APs in the central

adult SAN cells [2, 3].As this simulation result shows, in the neonate, it has a secondary contribution of automaticity. The greater $I_{Ca,L}$ current density in the neonate and the modulation of $I_{Ca,L}$ kinetics with age may play an important role in the high peak value of the APs in the neonate[5].

The present study also demonstrated an association between the age-dependent difference in current density and the $V_{1/2}$ of the I_f activation curve, which also contribute to a slowing down of the pacemaking rate in the adult. Previous studies[6][7] demonstrated that the pacemaker current I_f, exhibited an age-dependent decrease in current density which was assumed to result from baseline cAMP reduction levels in the SA node, suggesting that the combined action between I_f channels and fewer cAMP molecules are the main cause of the activation curve shift towards hyperpolarisation in older age groups, leaving fewer I_f channels available to initiate diastolic depolarisation, a key determinant of the heart rate decrease of the SA node.

The contribution of the delayed rectifier K^+ currents and Na^+/Ca^{2+} exchange current to SAN pacemaking in adult have been studied[12], but the role of developmental changes in potassium currents in the sinus node remains unexplored. Based on gene expression level measurements, the great abundance of I_{Kr}, I_{Ks} and I_{NaCa} in neonate SAN was of small consequence on the pacemaking effect.

In conclusion, this simulation study provided a novel computational model of the action potentials in neonate rabbit SAN cells, which is useful to generate novel predictions regarding the key differences between the ion channel currents mechanism as contributors to the fast heart rate in neonatal cellular physiology.

Acknowledgements

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