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Optimization of the ⁷Li(p,n) Proton Beam Energy for BNCT Applications

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ABSTRACT

The reaction ${}^{7}\text{Li}(p,n){}^{7}\text{Be}$ has been proposed as an acceleratorbased source of neutrons for Boron Neutron Capture Therapy (BNCT). This reaction has a large steep resonance for proton energies of about 2.3 MeV which ends at about 2.5 MeV. It has generally been accepted that one should use 2.5 MeV protons to get the highest yield of neutrons for BNCT. This paper suggests that for BNCT the optimum proton energy may be about 2.3 MeV and that a proton energy of about 2.2 MeV will provide the same useful neutron fluence outside a thinner moderator as the neutron fluence from a 2.5 MeV proton beam with a thicker moderator.

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Introduction

Boron Neutron Capture Therapy (BNCT) is a treatment modality for cancer that depends on an uptake of boron by tumor cells and then the exposure of these boronloaded tumor cells to thermal neutrons. This treatment is particularly promising for deep-seated brain tumors which are inoperable. The reaction ${}^{10}B(n,\alpha)^{7}Li$ produces high LET products whose ranges are roughly equivalent to the diameter of cancer cells (10 μ m). Interest in BNCT has been renewed due to research into a new generation of boronated drugs which show a selectively high uptake in animal tumors. For example a recent study by Hill¹ has measured selective tumor uptakes of boronated protoporphyrin (BOPP) as high as 400:1 relative to normal brain blood concentrations in mice.

Blue and collegues²⁻⁴ have published a great deal of work on accelerator-based BNCT facilities. The majority of accelerator-based BNCT proposals to date involve 2.5 MeV protons incident on a metal ⁷Li target, utilizing the ⁷Li(p,n)⁷Be reaction to produce neutrons. These neutrons must be slowed down in energy, via a filter (moderator/reflector) assembly, by roughly 2-4 orders of magnitude for BNCT treatments since the neutron distribution from the target peaks in the energy range of 400 to 600 KeV in the forward direction. The generally accepted³ useful neutron energy range from the filter assembly for treating deep-seated tumors is 1 eV to 1 KeV. In this paper we examine the optimum proton beam energy for different moderator and reflector combinations to produce the best neutron charateristics for BNCT.

Neutron Source Characterization

The reaction ${}^{7}\text{Li}(p,n){}^{7}\text{Be}$ displays a large resonance in the forward direction around 2.3 MeV which extends to about 2.5 MeV. It has been generally accepted that to get the highest neutron yield for BNCT one should use a proton beam energy of 2.5 MeV. However this is a careful tradeoff between neutron yield and neutron spectrum from the target. Upon close examination of the ${}^{7}\text{Li}(p,n)$ cross sections⁵ it appeared that a proportionally large high-energy tail is produced as one increases the incident proton energy. It was decided that these tradeoffs were not completely apparent and that a careful examination was needed.

A fortran program[†] was written to calculate neutron double differential (angle and energy) distributions from the target as a function of incident proton beam energy. Liskien⁵ has derived center of mass best values for normalized Legendre coefficients for predicting cross sections for the ⁷Li(p,n)⁷Be reaction. For a given proton energy the cross section, as a function of center of mass angle, can be determined in the center of mass system by:

$$\frac{d\sigma}{d\omega}(\phi) = \frac{d\sigma}{d\omega}(0^{\circ}) \sum_{i} A_{i} P_{i}(\phi)$$
(1)

where A_i are the coefficients of the Legendre polynomials determined by Liskien and $P_i(\phi)$ are the Legendre polynomials as a function of center of mass scattered angle. The total cross section integrated over all angles is simply given by:

$$\sigma = 4\pi \left(\frac{d\sigma}{d\omega} \left(0^{\circ}\right)\right) A_{0} \tag{2}$$

The Legendre coefficients are normalized such that

$$\sum_{i} A_i = 1.0 \tag{3}$$

Transformation from center of mass system variables to laboratory system is determined by the following relation⁶

$$\cos\theta = \frac{\cos\phi + \rho}{\sqrt{1 + 2\rho\cos\phi + \rho^2}} \tag{4}$$

The program lipn.f is available via anonymous ftp at fubar.lbl.gov (IP 131.243.214.19).

where ρ is defined as

$$\rho = \frac{m_p}{m_n \sqrt{1 + \frac{m_p + m_n Q}{m_n E}}} \tag{5}$$

The relation between the center of mass cross section and the laboratory system cross section is given by⁶

$$\sigma(\theta) = \sigma(\phi) \frac{\left(1 + 2\rho \cos\phi + \rho^2\right)^{\frac{3}{2}}}{1 + \rho \cos\phi}$$
(6)

The neutron energy is determined by the following relation⁷

$$E_n = E_p \frac{m_p m_n}{(m_n + m_r)^2} \left\{ 2\cos^2\theta + \frac{m_r (m_r + m_n)}{m_p m_n} \left[\frac{Q}{E_p} + \left(\frac{1 - m_p}{m_r} \right) \right] \\ \pm 2\cos\theta \sqrt{\cos^2\theta + \frac{m_r (m_r + m_n)}{m_p m_n}} \left[\frac{Q}{E_p} + \left(\frac{1 - m_p}{m_r} \right) \right] \right\}$$
(7)

where E_n and E_p are the neutron and proton kinetic energies, m_n and m_p their respective masses, m_r the target residual mass (*i.e.*⁷Be). The Q value for this reaction is given as⁵1.644 MeV. The reaction thresholds are given by Liskien as 1.881 MeV in the forward direction and 1.920 MeV in the backward direction. In our program the threshold, which is used to determine the target thickness, is assumed to be 1.950 MeV as this is as low as Liskien's Legendre coefficients were fitted to experimental data.

Only the reaction ${}^{7}\text{Li}(p,n){}^{7}\text{Be}$ is considered. The reaction ${}^{7}\text{Li}(p,n){}^{7}\text{Be}^{*}$ which produces a 0.431 MeV gamma with a threshold of 2.373 MeV in the forward direction and 2.423 MeV in the backward direction, and the reaction ${}^{7}\text{Li}(p,n){}^{7}\text{Be}^{**}$ which produces a 4.55 MeV gamma with a threshold of 7.08 MeV are not considered in our treatment. These cross sections are generally only a few percent of the ${}^{7}\text{Li}(p,n){}^{7}\text{Be}$ cross section at proton energies less than or equal to 2.5 MeV. In addition the breakup reaction ${}^{7}\text{Li}(p,n{}^{3}\text{He}){}^{4}\text{He}$ with a threshold at 3.692 MeV is not considered.



Figure 1: ⁷Li metal target thickness as a function of incident proton kinetic energy.

The target thickness is calculated by subtracting the range of the incident proton from the range of a proton at the threshold energy in Li metal. In this way only protons with energies at or above the reaction threshold are allowed to deposit any energy directly in the target to minimize heating of the target. Range and stopping power data are taken from Janni⁸ with log-log interpolation for intermediate energy values. Target thickness calculated by this program for various incident proton kinetic energies is shown in Fig. 1.

The target is then subdivided into 100 equal thickness subregions. In each region the sampled stopping power is used to determine the current proton beam energy, the Legendre coefficients are sampled and then the cross sections are determined according to Eqs. (1) and (6) over 1° angle increments. For each subregion a check is made to ensure that

$$\sigma = \int_{0}^{2\pi} \int_{0}^{\pi} \frac{d\sigma}{d\omega_L} = \int_{0}^{2\pi} \int_{0}^{\pi} \frac{d\sigma}{d\omega_C} = 4\pi \left(\frac{d\sigma}{d\omega}\right) (0^\circ) A_0 \tag{8}$$

where $d\omega_L$ and $d\omega_C$ are the lab system and center of mass system differential solid angles.



Figure 2: Differential neutron yields for protons on ⁷Li metal target.

For each proton energy and each sampled angle the neutron energy is calculated from Eq. (7). From this the overall double differential neutron production probabilities can be estimated for each incident proton beam energy from the accelerator. These are shown in Fig. 2.

The neutron energy spectra for various angle bins and for various incident proton kinetic energies are shown in Fig. 3. This information is used as the starting point for subsequent simulations of neutron transport in various moderator and reflector materials. Total neutron yields, integrated over all neutron energies and angles, are shown in Table 1.



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Figure 3: Neutron yields (per incident proton) as a function of neutron energy for different angle bins and various incident proton kinetic energies for the $^{7}Li(p,n)^{7}Be$ reaction.

E_p (MeV)	Yield (n/p)
2.1	2.69×10^{-5}
2.2	5.45×10^{-5}
2.3	9.26×10^{-5}
2.4	1.23×10^{-4}
2.5	1.46×10^{-4}
2.6	1.68 × 10 ⁴

Table 1: Total neutron yield as a function of incident proton energy (neutrons/incident proton).

Moderator Design and Modeling

To be useful in BNCT applications, the neutron spectra portrayed in Fig. 3 must be moderated sufficiently such that a maximum flux of useful epithermal neutrons is delivered to the patient while the dose due to non-useful neutrons is minimized. Several designs for beam shaping assemblies have been proposed for use in optimizing neutron beam characteristics for BNCT. These designs are normally optimized to deliver the best neutron spectra for a given 2.5 MeV proton incident beam. Such designs must be modified for lower energy proton beams, as the lower neutron energies produced in the ⁷Li(p,n)Be reaction need less moderation. Other factors, such as the reflector and beam delimiter configuration, normally do not need to be altered as their effect is largely independent of neutron energy.

The effect of changing the proton beam energy was analyzed on four different moderator designs, three of which have been proposed by $Blue^{3,4}$ and one by Greenspan⁹. The basic assembly designs, which consist of a moderator, reflector, and beam delimiter, are shown in Fig. 4. The difference in these designs is primarily in the choice of moderator. These choices are listed in Table 1, along with the optimum moderator thickness for 2.5 MeV protons, as determined by the designer.

The BeO design³ was orginally determined to provide the best moderation for BNCT effective neutrons. It was discarded for practicality and materials issues for a design based on heavy water, which could produce similar, though less optimal,

Configuration optimized for 2.5 MeV p's # Designed by Moderator Blue³ BeO 20.0 cm BeO, Al₂O₃ reflector 3 Blue^d 25.0 cm D₂O, Al₂O₃ reflector D_2O 2 3 Greenspan⁹ 7LiF/Pb 30.0 cm ⁷LiF, 1.0 cm Pb, Al₂O₃ refl. Blue⁴ 25.0 cm D₂O, ⁷Li₂CO₃ reflector 4 D_2O 30.0 cm diameter moderator 26.0 cm diameter accelerator beam port

Table 2: Various moderator/reflector designs considered for optimization in this work.

results. The ⁷LiF/Pb design⁹ was optimized by a one-dimensional transport code and did not originally include a reflector or beam delimiter, which were added in order to effectively compare it to the other designs. The final design by Blue⁴ effects some modifications due to recent work, such as a ⁷Li₂CO₃ reflector, which produces fewer capture gamma rays than Al₂O₃, and a wider beam port and moderator to accomodate target heating problems. There are small structural differences between this model and Blue's final design. The general reflector and beam delimiter geometry were not changed from the first three models in Table 2, so as to make more accurate comparisons between this and the other designs, based only on the change in materials and moderator geometry.

These four assemb were modeled using MCNP4¹⁰, a three dimensional, pointwise continuous cross-section Monte Carlo neutron/photon transport code to determine the optimum moderator thickness for each incident proton energy. ENDF/ B-V cross section data is used. MCNP's use of "point-wise continuous crosssections" means that linear interpolation between cross section data points over the entire energy range will reproduce the experimental cross section data to within 1%. The entire neutron source distribution mentioned earlier was modeled in 10° angle increments from 0° to 180° (azimuthally symmetric), with a distribution of 50 energy bins in each angle bin. In modeling the assembly, the thickness of the moderator was allowed to vary and for each thickness, the neutron flux spectrum in air at the patient window was determined.



Figure 4: Configurations of four design assemblies considered here. These are cross-sections of cylindrical assemblies. Proton beam enters from the top of the assembly. Each design consists of a moderator, reflector and a $D_2O/^6Li$ neutron shield around the reflector. The moderator thickness ("x") is allowed to vary.

It is difficult to judge the effectiveness of a particular neutron spectrum in air for use in BNCT applications. The assembly designs that were developed by Blue and evaluated here were optimized by Blue using a parameter known as the RUFTED (Ratio of Useful Fluence to Equivalent Dose), a parameter that we also use to determine the quality of a neutron fluence. The RUFTED is defined as:

$$RUFTED = \frac{\Phi_u}{K_n \cdot RBE_n + K_\gamma}$$

Here, Φ_u is the useful neutron fluence in n/cm²-source neutron, K_{γ} is the gamma kerma in cGy/source neutron, Kn is the neutron kerma is cGy/source neutron, and RBE_n(E) is the energy dependent neutron RBE (Relative Biological Effectiveness). The definition of the range of neutrons useful for BNCT is a matter of some debate and depends on many factors including tumor depth and Boron loading in the tumor and in normal tissue. It is generally accepted that 1eV is an appropriate lower limit, with some considerable debate on the upper limit^{11,3}. For our calculations, Φ_u has been defined as the fluence of neutrons at the irradiation point in the range of 1 eV-10 keV. Some testing has assured that the relative results in this paper are largely invariant to the exact definition of this range.

Of even greater debate than Φ_u is the debate over the definition of the neutron RBE. The energy dependent values given by Blue¹² were used here (see Fig. 5), as other choices only included distributions in inappropriate ranges¹³ for our purposes, or energy independent, constant values, which varied from 2 to 4. The questionable nature of the neutron RBE leads to uncertainty of its effect on our results and therefore we also analyzed the effect of using a constant neutron RBE of 2. Again, the relative results did not significantly differ and our conclusions were unchanged.

 Φ_u is also an important parameter in optimizing a particular assembly design. Φ_u , however, is a measure of the useful neutron fluence per source neutron. This should be normalized to the neutron yield per proton current, as lower energy protons at a given current will not yield as many source neutrons per second in the ⁷Li(p,n)Be reaction, as shown in Table 2. Additionally, because a larger proton



Figure 5: Neutron energy dependent RBE from Blue (REF) normalized to produce an energy-averaged RBE of 3.

flux can be used at lower energies, this parameter should also be normalized to the energy of the protons, making the optimization parameter $\Phi_{u/P}$ the useful fluence per accelerator power in units of n/cm²-s-kW:

$$\Phi_{u/P} = \Phi_u / \left(E_p \times Y \right)$$

where Ep is the energy of the proton in MeV and Y is the neutron yield per mA of incident protons on the lithium target. When testing the advantage of different assembly designs at variable proton energies, for a given constant RUFTED, one would ideally prefer the highest possible useful fluence per accelerator power. Or, for a given constant $\Phi_{u/P}$, one would prefer the highest possible RUFTED.

Each assembly was modeled using MCNP and the parameters RUFTED and $\Phi_{u/P}$ were calculated from the neutron flux energy spectrum at the irradiation point, 3 cm from the front of the beam port. The dose components of RUFTED were calculated by folding neutron and gamma fluences with ICRU-44 adult (M) average soft tissue kerma factors¹⁴ at the irradiation point. As previously described, the entire angle and energy dependent neutron distribution from the Lithium target is used in the MCNP model of the neutron source. This was done for different incident proton energies between 2.1 MeV and 2.7 MeV. For each energy on each assembly design, different moderator thicknesses were modelled to determine the RUFTED and $\Phi_{u/P}$ at each proton beam energy as a function of moderator thickness. Finally, graphs of RUFTED and $\Phi_{u/P}$ vs. moderator thickness were plotted for each proton beam energy. Two of these graphs are



Figure 6: RUFTED & $\Phi_{u/P}$ vs. moderator thickness, BeO moderator (Assembly design #1). 2.5 MeV incident protons are shown on the left and 2.3 MeV protons on the right.

shown in Fig. 6. From these graphs, the exact moderator thickness necessary for a particular parameter value (RUFTED or $\Phi_{u/P}$) can be determined, as well as

the value of the other parameter. A constant value of each parameter can then be taken to determine the effect of proton beam energy on the other parameter.

Each assembly design has already been optimized by the authors for protons at 2.5 MeV. For instance, Blue² has determined that 20.0 cm is the optimum BeO moderator thickness for design #1 at 2.5 MeV, taking into account the relative tradeoffs between RUFTED gain and $\Phi_{u/P}$ loss with increasing thickness. The RUFTED and $\Phi_{u/P}$ at this thickness can be read from the left plot of Fig. 6 and are found to be 5.63×10^9 n/(cm^{2*}cSv) and 4.69×10^9 n/(cm^{2*}s*kW), respectively. If each of these parameters is left constant, the value of the corresponding parameter at 2.3 MeV can be determined from the appropriate moderator thickness in the right side of Fig. 6. A constant RUFTED of 5.63×10^9 n/(cm^{2*}cSv) is acheived with only a 16.1 cm BeO moderator at 2.3 MeV, resulting in a higher $\Phi_{u/P}$ of 5.65×10^9 n/(cm^{2*}s*kw). Similarly, to acheive a constant $\Phi_{u/P}$ of 4.69×10^9 at 2.3 MeV, a 15.1 cm BeO moderator is needed, resulting in a higher RUFTED of 6.92×10^9 n/(cm^{2*}cSv).

Such an improvement in beam quality can be seen by comparing the energy spectra of each neutron beam at the irradiation point for these two different configuations. The increase in the number of useful neutrons for a given RUFTED and accelerator power is shown in Fig. 7^{\dagger} , which contains two histograms of neutron spectra as a function of energy for equal RUFTEDs with 2.5 MeV and 2.3 MeV incident protons. Again, this figure applies to assembly design #1, which contains a BeO moderator.

When $\Phi_{u/P}$ is taken as constant, the effect of a higher RUFTED is a lower unwanted patient dose. The energy-dependent contributions to dose from both neutrons and photons (created by neutron reactions in the assembly) for a constant $\Phi_{u/P}$ is shown in Fig. 8.

[†] All semi-log plots in this paper use 5 equal logarithmic intervals per decade to preserve spectral shape. Fluence values on these plots have not been divided by this interval (0.2) and therefore should not be multiplied by this interval when integrating.



Figure 7: Neutron fluence, Φ_n vs. energy for 2.3 MeV protons with 16.1 cm BeO moderator and 2.5 MeV protons on 20.0 cm BeO moderator.[†]

Note that lower energy protons also result in a lower photon dose to the patient, since fewer neutrons are initially neccessary in the smaller moderator to create the same useful fluence at the irradiation point. Thus, the fewer neutrons transporting through the assembly result in fewer (n,γ) reactions. Additionally, even though many of the higher energy neutrons are moderated to lower energies in the beam shaping assembly (for example, note the fast neutron spectra in Fig. 7), the primary contribution to the total dose to the BNCT patient is due to these fast neutrons. The primary advantage to a lower energy proton beam is the decreased production of these fast neutrons which contribute most of the dose to patient.

This analysis of a particular assembly can be expanded to include many different proton energies. By graphing the values of a single parameter (RUFTED or $\Phi_{u/P}$) while the other is left constant for a range of proton energies, the optimum proton



Figure 8: Neutron and gamma dose from BeO moderator design assembly #1 as a function of energy for 2.3 MeV incident protons (solid) and 2.5 MeV protons (dots). The difference between the two incident proton energies for the low energy "bump" due to thermal neutrons, and the high energy peak due to gammas, cannot be discerned.

energy can be determined. The values of each of these parameters as a function of incident proton energy for assembly design #1 is shown in Fig. 9.

The optimum accelerator energy is the value at which these parameters are at a maximum. While the two maxima do not exactly coincide, they do not differ much, indicating that the optimum proton energy for an assembly such as this is in the range of 2.3 MeV to 2.35 MeV, not 2.5 MeV, which has previously been popularly assumed to be the optimum operating accelerator energy. Additionally, an even lower energy of 2.2 MeV results in parameters similar to those at 2.5 MeV. This indicates that a BNCT design that ordinarily requires a 2.5 MeV accelerator can use a 2.2 MeV accelerator with little change in beam quality, or a 2.3 MeV accelerator with better beam quality.



Figure 9: RUFTED & $\Phi_{u/P}$ vs. moderator thickness, 20 cm BeO moderator (Assembly design #1) for various proton energies. For RUFTED values the $\Phi_{u/P}$ was held constant at 4.69×10^9 (n/cm²-s-kw). For $\Phi_{u/P}$ values the RUFTED was held constant at 5.63×10^9 (n/cm²-RBE*cGy).

Similar results are found when the same procedure is used to determine the optimum proton energy for other assembly designs. Fig. 10, Fig. 11 and Fig. 12 show the RUFTED and $\Phi_{u/P}$ as a function of proton energy for assemblies #2- #4, respectively.

These results are useful primarly as a rough estimate of the optimum proton energy for each assembly design. Both assembly designs #1 and #2 appear to function best at accelerator energies of near 2.3 MeV, with a sharp drop in beam effectiveness below this energy.

Assembly design #3, which consists primarily of a ⁷LiF moderator with 1 cm of lead at the end of the assembly near the irradiation point, does not show the same peak in beam effectiveness at 2.3 MeV. Instead, a peak occurs at 2.6 MeV. Additionally, this design can be used with lower beam energies down to 2.3 MeV



Figure 10: RUFTED & $\Phi_{u/P}$ vs. moderator thickness, D₂O moderator (Assembly design #2). For RUFTED values the $\Phi_{u/P}$ was held constant at 4.13×10^9 (n/cm²-s-kw). For $\Phi_{u/P}$ values the RUFTED was held constant at 4.75×10^9 (n/cm²-RBE*cGy).

- 2.35 MeV before significant losses in beam effectiveness occur. There are several difficulties involved in the analysis of this particular assembly design, however. First, assembly #3 contains two material zones. In simulations, only the thickness of the ⁷LiF was varied. The thickness of lead was left constant at 1 cm. Therefore, the exact configurations may not have been properly optimized for each proton energy, with error becoming more pronounced at lower proton energies, where much smaller moderator thicknesses are required.

A second more general concern is that the method of optimizing a BNCT neutron beam with a parameter such as the RUFTED is not ideal. A proper treatment would involve modeling the transport of the resultant neutron beam through a BNCT-treated phantom head. Unfortunately, additional factors would become prevalent, such as the tumor depth, the boron loading in tumor, the boron loading



Figure 11: RUFTED & $\Phi_{u/P}$ vs. moderator thickness, ⁷Li/Pb moderator (Assembly design #3). For RUFTED values the $\Phi_{u/P}$ was held constant at 4.77×10^9 (n/cm²-s-kw). For $\Phi_{u/P}$ values the RUFTED was held constant at 6.02×10^9 (n/cm²-RBE*cGy).

in healthy tissue, and the tumor size. A simple analysis of the value of a particular neutron beam would become tedious. Such an analysis is, however, eventually necessary, as the RUFTED does not always take into account major differences in the particular shapes of neutron beams produced by a specific moderator. Figure 13 shows the different neutron spectra of two beams produced by two different assembly designs (#1 and #3) which have equal $\Phi_{u/P}$'s and both spectrums are produced by 2.5 MeV incident protons. The spectrum produced by assembly #3 is more energetic with a higher percentage of fast neutrons within the useful fluence range of 100 eV - 10 keV as is shown in Fig. 13.

Finally, assembly design #4, which is similar in construction to assembly design #2 with differences in the reflecting medium, shows a similar behavior with



Figure 12: RUFTED & $\Phi_{u/P}$ vs. moderator thickness, D₂O moderator (Assembly design #4). For RUFTED values the $\Phi_{u/P}$ was held constant at 2.15×10^9 (n/cm²-s-kw). For $\Phi_{u/P}$ values the RUFTED was held constant at 3.35×10^9 (n/cm²-RBE*cGy).

changing proton energy as assemblies #1 and #2. The main differences are a less pronounced effect and a slightly shifted and broadened peak, centered instead at around 2.35 MeV. Again, it is apparent that 2.5 MeV is not necessarily the optimum energy at which to operate a proton accelerator.

The optimal designs for each assembly have been listed in Table 3, along with the percent improvement that can be realized in either RUFTED or $\Phi_{u/P}$, compared to performance at 2.5 MeV.

This paper has demonstrated the possibility that one may achieve either higher or comparable useful neutron fluxes and beam qualities at energies lower than the often accepted value of 2.5 MeV. To verify this better figures of merit than the $\Phi_{u/P}$ and RUFTED should be found that can be used to compare spectra oudside



Figure 13: Neutron spectral shape for assembly designs #1 (BeO moderator by Blue) and #3 (⁷Li/Pb by Greenspan). The Φ_n is identical in both cases and is equal to 1.3×10^{-4} (n/cm²-s-proton). Both spectrums are produced from incident 2.5 MeV proton beams.

the moderator port without having to perform detailed patient treatment planning for each design parameter change and patient/turnor configuration.

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r	Assembly	RUFTED	Φ /P	% Increase in Given Quantity
[Design	(n/cm ² -RBE-cGy)	(n/cm^2-s-kW)	Over Reference Design
#1	2.5 MeV			
<i>"</i> -	20.0 cm BeO	5.62×10^{9}	4.69×10^{9}	(Reference $\#1$)
				······································
#1	2.3 MeV	Í	ĺ	
	16.3 cm BeO	5.64×10^{9}	5.59×10^{9}	$19.2\% \Phi_{u/P}$
		· · · · · · · · · · · · · · · · · · ·		
#1	2.3 MeV			
	17.2 cm BeO	6.81×10^{9}	4.74×10^{9}	21.2% RUFTED
#2	2.5 MeV			
	25.0 cm BeO	4.75×10^{9}	4.13×10^{9}	(Reference #2)
#2	2.3 MeV			
	20.8 cm BeO	4.69 × 10 ⁹	4.72×10^{9}	14.4% Φ _{u/P}
#2	2.3 MeV	0	.0	
	21.8 cm BeO	5.30 x 10 ⁹	4.10×10^{9}	11.6% RUFTED
#3	2.5 MeV	0.00 109		(7) (10)
	30.0 cm 7LaF	$6.02 \times 10^{\circ}$	4.76 × 10°	(Reference #3)
""	2010-11			
7 #-3	2.0 MeV	6 00 × 10 ⁹	E 10 × 10 ⁹	7197 đ
	31.8 CH /LIF	0.00 X 10-	5.10 × 10	7.1% Ψu/P
42	2.6 MeV			
~~	32.6 cm 7L/F	6 55 v 10 ⁹	4 75 × 10 ⁹	8 8% BUFTED
	02.0 CHI 1011	0.30 × 10	4.10 × 10	0.070 1007 120
#4	2.5 MeV			
7	25.0 cm D2O	3.38×10^{9}	2.15×10^{9}	(Reference #4)
				······································
#4	2.35 MeV			
	22.3 cm D2O	3.35×10^{9}	2.39×10^{9}	$11.1\% \Phi_{u/P}$
				·
#4	2.35 MeV			
	23.0 cm D2O	3.70×10^{9}	2.14×10^{9}	9.5% RUFTED

References

- J. S. Hill *et al.*, "Selective Tumor Uptake of a Boronated Porphyrin in an Assimal Model of Cerebral Glioma", Proceedings of the National Academy of Sciences of the United States of America, 89(5), 1785-1789 (1992).
- J. W. Blue et al., "A Study of Low Energy Proton Accelerators for Neutron Capture Therapy", proc. 2nd Int. Symp. Neutron Capture Therapy, October 18-21, 1985, pg. 147, H. Hatanaka, Ed., Nishimura Co., Ltd. (1985).
- C. K. Wang, T. E. Blue and R. Gahbauer, "A Neutronic Study of an Accelerator Based Neutron Irradiation Facility for Boron Neutron Capture Therapy", Nuclear Technology Volume 84, 93-107 (1989).
- N. Gupta "Fabrication and Preliminary Testing of a Moderator Assembly for an Accelerator-Based Neutron Source for Boron Neutron Capture Therapy", PhD Thesis, Ohio State University (1995).
- H. Liskien and A. Paulsen, "Neutron production Cross Sections and Energies for the Reactions ⁷Li(p,n)⁷Be and ⁷Li(p,n)⁷Be*", Atomic Data and Nuclear Data Tables, 15, 57-84 (1975).
- Herbert Goldstein <u>Classical Mechanics</u>, Addison Wesley Publishing Company (1980).
- 7. K. H. Beckurts and K. Wirtz, <u>Neutron Physics</u>, Springer-Verlag (1964).
- J. F. Janni, "Proton Range-Energy Tables, 1 KeV 10 GeV", Atomic Data and nuclear Data Tables, Volume 27, Numbers 4/5, July/September (1982).
- Y. Karni et al., "Optimal Beam-Shaping Assemblies for BNCT Facilities", Proceedings of the American Nuclear Society Meeting, November (1995), San Francisco.
- "MCNP-A A General Monte Carlo N-Particle Transport Code, Version 4A," LA-12625, J. F. Briesmeister, Ed., Los Alamos National Lab. (1993).

- J. C. Yanch, X-L. Zhou and G. L. Brownell, "A Monte Carlo Investigation of the Dosimetric Properties of Monoenergetic Neutron Beams for Neutron Capture Therapy", Radiation Research 126, 1-20 (1991).
- T. E. Blue, J. E. Wollard and N. Gupta, "Neutron RBE as a Function of Energy", Proceedings of the 8th International Conference on Radiation Shielding, April 24-28 (1994) Arlington, Texas, published by the American Nuclear Society.
- E. L. Alpen and K. A. Frankel, "Biological Effectiveness of Recoil Protons from Neutrons of Energy 5 keV to 5 MeV", Advances in Neutron Capture Therapy, Edited by A. H. Soloway et al., Plenum Press, New York (1993).
- "Photon, Electron, Proton and Neutron Interaction Data for Body Tissues", ICRU Report 46, February 28 (1992).